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2

3 **Title:** Development of an anthropometric prediction model for fat free mass and muscle mass in
4 elite athletes

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16 **Running Title:** Anthropometric models for lean mass tissues

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26 **ABSTRACT**

27 The monitoring of body composition is common in sports given the association with performance.
28 Surface anthropometry is often preferred when monitoring changes for its convenience,
29 practicality and portability. However, anthropometry does not provide valid estimates of absolute
30 lean tissue in elite athletes. The aim of this investigation was to develop anthropometric models
31 for estimating fat free mass (FFM) and skeletal muscle mass (SMM) using an accepted reference
32 physique assessment technique. Sixty-four athletes across eighteen sports underwent surface
33 anthropometry and dual-energy X-ray absorptiometry (DXA) assessment. Anthropometric models
34 for estimating FFM and SMM were developed using forward selection multiple linear regression
35 analysis and contrasted against previously developed equations. Most anthropometric models
36 under review performed poorly compared to DXA. However, models derived from athletic
37 populations such as the Withers equation demonstrated a stronger correlation with DXA estimates
38 of FFM ($r=0.98$). Equations that incorporated skinfolds with limb girths were more effective at
39 explaining the variance in DXA estimates of lean tissue (Sesbreno FFM ($R^2 = 0.94$) and Lee SMM
40 ($R^2 = 0.94$) models). The Sesbreno equation could be useful for estimating absolute indices of
41 lean tissue across a range of physiques if an accepted option like DXA is inaccessible. Future
42 work should explore the validity of the Sesbreno model across a broader range of physiques
43 common to athletic populations.

44

45 **INTRODUCTION**

46 The assessment of body composition is common in sports given the association with performance.
47 In many elite sport programs, fat mass (FM) is monitored given the negative implications of
48 excessive fat on power to weight ratio, hydrodynamic drag, and performance scores (Claessens et
49 al., 1994; Claessens et al., 1999 & Siders et al., 1993). However, indices of lean tissue may also
50 have an important association with competitive success. (Slater et al., 2005 & Sanchez-Munoz, et
51 al., 2017). It is therefore important to examine body composition in elite athletes to assess their
52 relationship with performance in the field.

53 Dual Energy X-Ray Absorptiometry (DXA) is increasingly integrated into the monitoring of
54 athletic populations to provide timely information on both absolute and relative whole body and
55 regional body composition, plus bone health (Meyers et al., 2013). However, without careful
56 adherence to best practice guidelines, DXA precision error may fall beyond expected body
57 composition changes observed over a training period (Zemski et al., 2018a). Additionally,
58 radiation health regulations and/or equipment inaccessibility may restrict the use of DXA,
59 precluding frequent monitoring in some regions. This would limit the potential use of DXA to
60 better inform dietary and/or training interventions based on body composition changes observed.
61 Therefore, a complementary method like surface anthropometry would be useful.

62 Surface anthropometry is frequently used for monitoring body composition in athletes due to its
63 portability, cost effectiveness and extremely high precision (Meyer et al., 2013). A number of
64 skinfold equations have been validated to estimate body fat percent (BF%) (Forsyth et al., 1973,
65 Reilly et al., 2009; Thorland et al., 1984 & Withers et al., 2009), and through simple calculation,
66 absolute FM and fat free mass (FFM; overall mass excluding fat mass). Some practitioners apply
67 this approach of estimating FFM in athletes in the daily training environment. However, few, if
68 any of these skinfold equations have been validated to quantify body composition change (Cisar
69 et al., 1989; Silva et al., 2009 & Wilmore et al., 1970), and concerns have been raised about
70 inference of FFM from an indirect measure of subcutaneous FM (Martin et al., 1990). An
71 alternative approach would be to include a wider range of anthropometric measures as applied in
72 the Drinkwater fractionation model to estimate body composition (Drinkwater et al., 1980).

73 The Drinkwater four-way fractionation model uses the unisex phantom model to partition total
74 body mass into four compartments - FM, skeletal muscle mass (SMM; intramuscular adipose
75 tissue included), bone mass and residual mass (Drinkwater et al., 1980). This model may offer
76 some advantages for estimating FFM, lean body mass (LBM; overall mass excluding fat and bone
77 masses) and SMM compared to those exclusively derived from skinfolds. However, the effort to
78 optimize physique for performance has lead to a wide range of physique characteristics in elite
79 sports. This may limit the suitability of an anthropometric equation for evaluating body
80 composition across a range of sports. For instance, the fractionation model may not be
81 generalizable to muscular athletes as marked variance between total fractionated mass and scaled

82 mass have been observed in muscular individuals (Keogh et al., 2007). Therefore, other models
83 need to be considered for athletes across a range of physiques.

84 The present study aimed to: 1) compare the ability of selected anthropometric models to evaluate
85 lean tissues in elite athletes compared to DXA; & 2) develop an anthropometric prediction model
86 for FFM and SMM in elite Canadian athletes.

87

88 **METHODS**

89 *Recruitment*

90 Sixty-five athletes, 17 years of age or older, were recruited through emails sent to sport science
91 staff across the Canadian Olympic and Paralympic Sport Institute Network and National Sport
92 Organizations as well as poster marketing throughout the Canadian Sport Institute Ontario between
93 October 2017 and October 2018. Athletes were eligible for inclusion if they competed
94 internationally for Canada at a sport event hosted by an International Federation on the Olympic
95 program between October 2016 and October 2018. Athletes were provided with details on the
96 nature of the study, and all participants provided written informed consent in accordance with the
97 declaration of Helsinki. Ethics approval was obtained through the University of Stirling and the
98 Canadian Sport Institute Ontario Research Ethics Committees.

99 *Experimental Design*

100 Data collected included athlete demographics, urinalysis, pregnancy testing (Golden Time, One
101 Step, HCG Pregnancy Test 2.5mm strip) if female, anthropometry and DXA. Anthropometry and
102 DXA testing were conducted back to back on the same day. Subjects were excluded from the
103 study if they were >190cm tall. Female athletes were excluded if they were pregnant.

104 To minimize biological variability, all assessments were conducted in an overnight fasted (≥ 8
105 hours post-prandial), rested state following a low training volume day. Participants were instructed
106 to maintain their usual dietary habits the day prior to testing, with the addition of 500ml of water
107 at each eating occasion. To confirm hydration status, specific gravity of the first void urine sample
108 on the morning of testing was assessed using an automated refractometer (Atago 4410 Digital

109 Urine Refractometer, Tokyo, Japan). Those who were hypohydrated, as defined by a USG >1.026
110 (Armstrong et al., 2010 & Rodriguez-Sanchez et al., 2015) were excluded.

111 *Dual-Energy x-Ray Absorptiometry*

112 The DXA (Lunar Prodigy, GE Healthcare, Madison, WI) was calibrated with phantoms as per
113 manufacturer guidelines each day before measurement. All scans were conducted by the same
114 bone densitometry technologist (ES), certified through the International Society of Bone
115 Densitometry, with a within day repeated test-retest technical error of measurement of 0.4% for
116 total lean and 1.5% for total fat mass. The USA (Combined NHANES (ages 20-30) / Lunar (ages
117 20-40)) Total Body Reference Population (v113) was used as the reference database with analysis
118 performed using GE Encore version 13.60 software (GE, Madison, WI). The thickness mode was
119 determined by the auto scan feature in the software and all safety protocols as per the institution's
120 radiation safety protection plan were adhered to.

121 Athletes were asked to wear minimal clothing without metal zippers, tags, or studs and with all
122 metal jewelry removed. Athletes were positioned according to protocols previously described
123 (Nana et al., 2015). Athletes were centrally aligned on the scanning area with their head positioned
124 in the Frankfort plane and with their feet placed in custom-made radio-opaque polystyrene foam
125 blocks to maintain a constant distance of ~15cm between the feet. Similarly, the participants'
126 hands were placed in shaped polystyrene foam blocks, so they would be in a mid-prone position
127 with a consistent gap of ~3cm between the palms and trunk. Two Velcro straps were used to
128 minimise any participant movement during the scan. One strap was secured around the ankles
129 above the foot positioning pad and the other strap was secured around the trunk at the level of the
130 mid forearms. All scans were analysed automatically by the DXA software, but all regions of
131 interest were reconfirmed by the technician (ES) before being included in the subsequent statistical
132 analysis.

133 Appendicular lean soft tissue (ALST) derived from DXA was used to estimate SMM via the Kim
134 equation (Kim et al, 2002).

135 *Surface Anthropometry*

136 Full anthropometric profiles, including body mass, stretch stature, sitting height, skinfolds at eight
137 sites, eleven girths, nine lengths and six breadths were landmarked and measured by an

138 anthropometrist holding a level III accreditation from the International Society for the
139 Advancement of Kinanthropometry (ISAK) (ES) with a technical error of measurement of $\leq 2.0\%$
140 for sum of eight skinfolds and $\leq 1.0\%$ for all other measures.

141 Sitting height and stretch stature were measured using a wall mounted stadiometer (Perspective
142 Enterprises, Portage, Michigan, USA) with a precision of $\pm 1.0\text{mm}$. Skinfolds was assessed using
143 Harpenden calipers (Baty International, Burgess Hill, England). Girth measurements were
144 undertaken using a flexible steel tape (Rosscraft, Surrey, BC, Canada). Body limb lengths were
145 measured with a modified steel tape adapted with a segmometer (Rosscraft, Surrey, BC, Canada).
146 The majority of breadths were measured with the Campbell 20 large sliding bone caliper
147 (Rosscraft, Surrey, BC, Canada); biepicondylar breadths were measured with a Campbell 10 small
148 sliding bone caliper (Rosscraft, Surrey, BC, Canada). Body mass was assessed in minimal clothing
149 on a calibrated digital scale with a precision of $\pm 0.1\text{ kg}$ (Seca 876, Hamburg, Germany).

150 All measurements were made on the right side of the body using ISAK techniques previously
151 described (Stewart et al., 2011). All measurements were undertaken in duplicate. If the difference
152 between duplicate measures exceeded 5% for an individual skinfold or 1% for all other variables,
153 a third measurement was taken after all other measurements were completed. The mean of
154 duplicate or median of triplicate anthropometric measurements were used for all subsequent
155 analyse.

156 The fractionation (Drinkwater & Ross, 1980) and multiple linear regression models (Withers et al,
157 1987, Lee et al., 2000 & Reilly et al., 2009) were used to estimate body composition through
158 surface anthropometry (Table 1). The Siri equation (Siri, 1956) was used to convert body density
159 to percent body fat for the Withers' equation (Withers et al., 1987). For both the Reilly (Reilly et
160 al 2009) and Withers equations, FFM was calculated according to the following equation:

$$161 \text{ FFM (kg) = body mass (kg) - (body mass (kg) x body fat \% / 100).}$$

162 Fractionated muscle, fat, bone, and residual masses were calculated as previously described
163 (Drinkwater and Ross, 1980) and selectively combined to generate estimates of:

$$164 \text{ Fractionated FFM (kg) = fractionated SMM (kg) + fractionated residual mass (kg) + fractionated} \\ 165 \text{ bone mass (kg)}$$

166 Fractionated LBM (kg) = fractionated residual mass (kg) + fractionated SMM (kg)

167 The fractionated SMM and Lee equations (Lee et al., 2000) were used to predict SMM. ISAK
168 landmarks were used to operate the Lee equation to better manage time limitations in the
169 laboratory. The original landmarks for the Lee equation are approximately near 1cm of the ISAK
170 landmarks for each input variable, thus the differences associated with technical error of
171 measurement were assumed as minimal.

172 *Statistical Methods*

173 Statistical analyses were carried out using SPSS (SPSS v23.0; IBM Inc, Chicago, IL). Descriptive
174 statistics are presented as mean (μ) \pm standard deviation (SD). Differences in physique traits based
175 on gender were investigated using independent t-tests. Box plots and Q-Q plots were used to
176 identify any extreme outliers, with participants considered outliers if they were greater than two
177 SD away from all somatotype classifications.

178 A least square regression analysis was used to assess the validity of fractionated FFM, fractionated
179 LBM and fractionated SMM compared to DXA. The potential for any fixed bias was assessed by
180 determining whether the intercept for the regression was different from zero. The slope of the
181 regression line was used to identify proportional bias if it was different from one. Random error
182 was quantified using the standard error of the estimate (SEE) from the regression. Predictive
183 accuracy of the FFM, LBM and SMM equations were evaluated by calculating the mean 95%
184 prediction interval (M95%PI). This interval represents the uncertainty of predicting the value of
185 a single future observation.

186 Forward selection multiple regression analysis was performed using fractionated FFM and
187 fractionated FM from the elite Canadian athlete data set to derive a prediction model of FFM and
188 SMM for this population group. Data for the regression analysis conformed to the assumptions of
189 homoscedasticity, independent and normally distributed and no multicollinearity.

190

191 **RESULTS**

192 Sixty-five athletes across eighteen sports including beach volleyball, track cycling and athletics,
193 were recruited for the study. After preliminary statistical analysis, one athlete was removed from

194 the final analysis as the subject was identified as an extreme outlier, leaving sixty-four
 195 participants. Full anthropometric and body composition characteristics are presented in Tables 2
 196 and 3. Significant differences between male and female athletes were observed among bone
 197 breadths, upper body girths, upper limb girths and body composition parameters.

198 All anthropometric models for predicting FFM, LBM and SMM had a strong positive correlation
 199 with reference DXA measures (Table 4). The strength of correlation was similar amongst all
 200 anthropometric equations for FFM as well as between equations for SMM.

201 The slope, intercepts, standard error of the estimate and M95%PI for each anthropometric
 202 equation are listed in Table 4. Of all the FFM equations assessed, the random error and
 203 magnitude of the M95%PI were lowest with the Withers' equation. All equations overestimated
 204 FFM compared to DXA and varied in proportional bias. The degree of proportional bias was
 205 higher in female athletes. When examining the various fractionation models, the random error
 206 improved from FFM to SMM in all participants and across genders. Amongst the fractionated
 207 models, fractionated LBM had the highest random error, and M95%PI in all participants. The
 208 Withers' equation had the lowest M95%PI amongst the FFM models, whereas the fractionated
 209 SMM equation had the lower M95%PI between the SMM models in all participants. Between
 210 the fractionated and Lee equations for predicting SMM, the fractionated equation had a lower
 211 random error in all participants and female athletes. The Lee equation had the lowest fixed and
 212 proportional biases in all participants. The fractionated equation overestimated SMM in all
 213 subjects while showing proportional bias.

214 Forward selection multiple regression analysis was used on 64 athletes to derive 2 novel
 215 equations (Table 5). The equations are:

$$216 \quad \text{Sesbreno FFM (kg)} = 3.397 + (0.975 \times \text{Fractionated Fat Free Mass (kg)}) - (0.576 \times \\ 217 \quad \text{Fractionated Fat Mass (kg)})$$

$$218 \quad \text{Sesbreno SMM (kg)} = -2.485 + (1.058 \times \text{Fractionated Skeletal Muscle Mass (kg)}) - \\ 219 \quad (0.235 \times \text{Fractionated Fat Mass (kg)})$$

220 Using the combination of fractionated FFM and FM, the Sesbreno model explained 94% of the
 221 variance in DXA FFM compared to the Withers and Reilly equations, which explained 5% and
 222 32% of the variance, respectively. When using the combination of fractionated SMM and FM,

223 the Sesbreno model explained 93% of the variance in DXA SMM, while the Lee equation
224 explained 94%.

225

226 **DISCUSSION**

227 The primary finding of this investigation is that most anthropometric models for estimating
228 absolute indices of lean tissue performed poorly compared to DXA. The more effective options
229 were the Lee and novel Sesbreno equations, most likely because they were derived from
230 populations similar to the one being investigated. In this study, the highest correlation with
231 estimates of FFM from DXA was the Withers equation. This could be a function of using a
232 female athlete derived equation on a sample that was proportionally high in female athletes. This
233 would be consistent with work involving elite football athletes where equations derived from
234 athletic populations were superior at estimating absolute fat mass compared to estimates from
235 general population (Reilly et al., 2009). However, given morphological optimization, athletic
236 physiques may vary markedly and as such, sport specific regression equations may need to be
237 derived. For instance, the Reilly and Withers equations were derived from athletic populations,
238 and both demonstrated a greater tendency to deviate from DXA at the higher end of the range of
239 estimates of FFM. This parallels an earlier finding that described greater differences in total
240 body mass between the anthropometric fractionation model and the weight scale in more
241 muscular powerlifters (Keogh et al., 2007). Therefore, it may be important to account for the
242 athletic population when selecting an anthropometric model for estimating absolute indices of
243 lean tissue, but attention to the validity of the input variables may also be necessary.

244 The anthropometric models that complemented skinfold data with girth measurements, indirect
245 measures of lean tissues, were more suitable for estimating absolute indices of lean tissue. For
246 instance, the Sesbreno and Lee equations incorporated indirect measures of lean tissue, and both
247 performed similarly for estimating SMM. This confirms prior research involving human
248 cadavers that revealed a strong correlation between corrected limb girths and SMM (Martin et
249 al., 1990). Moreover, the Sesbreno model for estimating FFM was superior at explaining the
250 variance in DXA estimates of FFM compared to the Withers and Reilly skinfold equations. It
251 suggests that using a wide range of physique traits, and not skinfold alone, are important for
252 modeling indices of lean tissue in athletes. Learning the value of combining athletic population

253 characteristics with indirect measurements of lean tissues for the development of anthropometric
254 models, may help create practical and more suitable resources for practitioners to manage
255 evaluations in athletic populations.

256 Absolute estimates of lean tissue may be necessary for a range of reasons. While quantifying
257 absolute change in LM in response to training and/or nutrition is commonly advocated, estimates
258 of FFM may be necessary to interpret data related to resting metabolic rate (RMR) for the
259 assessment of energy availability (EA). For instance, the Sesbreno FFM model may be used to
260 operate the Cunningham equation (Cunningham, 1980) for estimating predicted RMR. When
261 interpreting a simulated calculation of predicted RMR on the smallest athlete in this
262 investigation, the agreement between DXA and the Sesbreno model (+0.8% difference) was
263 better compared to the Withers (+3.8%) and Reilly equations (+2.1%). Using the Sesbreno
264 model may reduce additional variance observed from using the skinfold equations and limit the
265 odds of overestimating cases of suppressed RMR from the assessment of measured:predicted
266 RMR for the detection of low energy availability. The Sesbreno model is likely appropriate for a
267 range of athlete sizes, but its suitability for very muscular athletes (FFM index >23.4 kg/m²) and
268 those standing taller than 190cm warrants investigation. If DXA is inaccessible, well selected
269 anthropometric models could allow practitioners to operate broader assessments for managing
270 athlete care, but may not have the precision to track small but important changes in response to
271 training and/or diet. The ability of the Sesbreno equation to accurately track changes in body
272 composition warrants investigation. However, before selecting any model for evaluating body
273 composition, it is important to recognize the limitations our investigation to inform assessment
274 outcomes.

275 Several decisions on study design impacted the assessment of indices of lean tissue. First, DXA
276 precision error is recognised to be impacted by an array of factors, including client presentation
277 (Nana et al., 2015 & Rodriguez-Sanchez et al., 2015). While guidance was provided to athletes
278 on ways of minimising this, responsibility for this was left with the athletes. However, upon
279 waking indices of hydration status confirmed all athletes presented in a euhydrated state.
280 Second, three athletes with titanium bone plates, or rods and screws inserted in the upper or
281 lower limb, were included in the study analysis. Titanium bone inserts, such as hip replacement
282 devices have shown to increase the risk of overestimating FFM when using DXA (Madsen et al.,

283 1999). However, the implants in our subjects were considerably smaller leading to assume that
284 the degree of inaccuracy was lower than reported. Third, the Kim equation was used for
285 estimating SMM from DXA results. The Kim equation required a DXA estimate of ALST, with
286 subject's hands in the prone position. Our subjects' were in the mid-prone position to manage
287 best practice protocols for body composition testing (Nana et al., 2015). A second scan was
288 avoided to better manage time restraints and exposure to radiation. Although variations in hand
289 position could result in a statistical difference in lean mass estimate of the limbs, the absolute
290 difference was expected to be small (<0.1kg) (Thurlow et al., 2017). Finally, the original
291 landmarking protocol for the Lee equation was replaced with the ISAK protocol to manage
292 restraints on time. It is unclear if the performance of the Lee equation was a function of the
293 regression model and/or errors associated with the estimates of indirect measures of lean tissue.
294 However, the variance in landmark points between the Lee and ISAK protocols was small and
295 unlikely resulted in a meaningful difference in girths and skinfolds measurements (Daniel et al.,
296 2010 & Humes et al., 2008). These incidences provide a reminder that avoiding protocols
297 specified in the original research introduces noise in the assessment.

298 In conclusion, carefully selected anthropometric models could be useful for estimating indices of
299 lean tissue if other assessment methods are inaccessible. Ideally, the model should be derived
300 from a similar population and from indirect measures of lean tissue. It is also advocated that the
301 practitioner uses landmarks consistent with the original study to minimize noise. Compared to
302 skinfold anthropometric models assessed, the novel Sesbreno equation may offer a suitable option
303 for estimating absolute indices of lean tissue to undertake broader assessments such as the
304 interpretations of resting metabolic rate or energy availability. Future work should explore the
305 validity of the Sesbreno model across a broader range of physiques common to athletic
306 populations.

307

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400 **Table 1. Anthropometric regression models assessed in this investigation**

Authors	Reference Assessment	Equation Input Variables
Drinkwater & Ross, 1980	Anthropometry	Fractionated FFM (kg) = standing height, biacromial breadth, biliocrystal breadth, transverse chest breadth, anterior-posterior chest depth, bi-epicondylar femur, bi-epicondylar humerus, wrist girth, ankle girth, corrected relax arm girth, forearm girth, corrected chest girth, corrected thigh girth and corrected calf girth.
		Fractionated SMM (kg) = standing height, corrected relax arm girth, forearm girth, corrected chest girth, corrected thigh girth and corrected calf girth.
		Fractionated FM (kg) = standing height, triceps skinfold, subscapular skinfold, supraspinale skinfold, abdominal skinfold, front thigh skinfold, and medial calf skinfold.
Withers et al., 1987	Hydrodensitometry	BF (%) = bicep skinfold, triceps skinfold, subscapular skinfold, supraspinale skinfold, abdominal skinfold, front thigh skinfold, and medial calf skinfold.
Reilly et al., 2009	DXA	BF (%) = triceps skinfold, mid-thigh skinfold and medial calf skinfold
Lee et al., 2000	MRI	SMM (kg) = standing height, corrected arm girth, corrected thigh girth, corrected calf girth, gender, age and race

402 **Table 2. Anthropometric characteristics of the elite Canadian athletes**

Variables		All N = 64		Male N = 20		Female N = 44		p value
		$\mu \pm SD$	Range	$\mu \pm SD$	Range	$\mu \pm SD$	Range	
Basics	Standing Height (cm)	174.3 \pm 6.9	156.9-188.3	179.6 \pm 5.0	171.5-188.3	171.9 \pm 6.3	156.9-182.9	0.000
	Body Mass (kg)	70.9 \pm 9.9	49.1-96.6	79.4 \pm 9.5	60.9-96.6	67.1 \pm 7.4	49.1-80.8	0.000
Skinfolds (mm)	Sum of 8	82.5 \pm 29.9	34.9-183.4	68.2 \pm 35.0	34.9-183.4	87.8 \pm 25.5	36.4-167.5	0.008
Girths (cm)	Arm Relax	30.1 \pm 3.3	23.1-38.3	32.6 \pm 3.4	26.4-38.3	29.0 \pm 2.5	23.1-36.0	0.000
	Arm Flexed	31.4 \pm 3.4	25.0-39.9	34.7 \pm 3.3	29.1-39.9	30.0 \pm 2.2	25.0-36.7	0.000
	Forearm	26.6 \pm 2.5	22.4-33.8	29.1 \pm 2.5	24.6-33.8	25.5 \pm 1.4	22.4-28.4	0.000
	Wrist	16.0 \pm 1.0	14.3-19.2	17.1 \pm 1.0	15.2-19.2	15.6 \pm 0.6	14.3-16.8	0.000
	Mesosternale	94.4 \pm 6.9	80.0-112.5	101.5 \pm 6.0	89.8-112.5	91.2 \pm 4.4	80.0-103.4	0.000
	Mid Thigh	55.4 \pm 4.2	46.4-66.4	56.5 \pm 4.6	49.2-66.4	54.9 \pm 3.9	46.4-63.6	0.299
	Calf Maximum	36.7 \pm 2.1	31.5-42.6	37.3 \pm 2.1	34.5-42.6	36.4 \pm 2.0	31.5-41.0	0.154
	Ankle	22.4 \pm 1.3	19.1-22.4	23.2 \pm 1.3	20.9-25.7	22.0 \pm 1.1	19.1-24.2	0.003
Breadths (cm)	Bioacromial	39.2 \pm 2.2	34.8-46.5	41.3 \pm 1.8	38.9-46.5	38.2 \pm 1.7	34.8-41.9	0.000
	Biiliocristale	28.2 \pm 1.6	24.1-32.1	28.5 \pm 1.4	26.2-31.7	28.2 \pm 1.8	24.1-33.2	0.000

	Transverse Chest	28.7±2.2	25.5-34.3	31.1±1.8	27.0-34.3	27.8±1.9	25.5-35.4	0.000
	A-P Chest	18.4±1.8	14.2-22.4	20.1±1.5	17.1-22.4	17.8±1.8	14.2-25.2	0.000
	Humerus	6.8±0.5	5.8-7.9	7.3±0.4	6.3-7.9	6.5±0.3	5.8-7.2	0.000
	Femur	9.4±0.5	8.2-11.0	9.9±0.5	9.1-11.0	9.2±0.4	8.2-10.3	0.000

403 Data are Mean (μ) \pm Standard Deviation (SD); Sum of 8 skinfolds=bicep, subscapular, tricep, iliac, supraspinale, abdominal, front

404 thigh and mid-calf; A-P = anterior-posterior.

405 **Table 3. Physique characteristics of the elite Canadian athletes**

Body Composition	Method	All N=64		Male N=20		Female N=44		p value
		$\mu \pm SD$	Range	$\mu \pm SD$	Range	$\mu \pm SD$	Range	
Fat Free Mass (kg)	DXA	57.9 \pm 9.0	49.7-97.4	67.7 \pm 7.5	55.4-80.2	53.4 \pm 5.2	42.4-63.8	0.000
	Fractionation (1980)	60.4 \pm 9.0	43.7-77.9	70.3 \pm 6.9	56.3-77.9	55.9 \pm 5.6	43.7-67.3	0.000
	Withers (1987)	61.9 \pm 8.7	45.3-83.0	70.9 \pm 7.5	57.6-83.0	57.9 \pm 5.5	45.3-69.5	0.000
	Reilly (2009)	61.9 \pm 8.6	44.2-83.2	70.5 \pm 7.6	56.2-83.2	58.0 \pm 5.8	44.2-69.6	0.000
Lean Body Mass (kg)	DXA	54.8 \pm 8.7	39.8-76.5	64.2 \pm 7.3	52.6-76.5	50.5 \pm 5.0	39.8-60.6	0.000
	Fractionation (1980)	49.6 \pm 7.2	35.6-64.1	57.5 \pm 5.6	46.4-64.1	46.1 \pm 4.6	35.6-55.2	0.000
Skeletal Muscle Mass (kg)	DXA	29.6 \pm 5.6	19.8-43.3	35.6 \pm 5.0	27.1-43.3	27.2 \pm 3.7	19.8-36.8	0.000
	Fractionation (1980)	32.1 \pm 5.1	22.1-42.2	37.5 \pm 4.2	29.7-43.0	29.7 \pm 3.2	22.1-36.2	0.000
	Lee (2000)	29.6 \pm 5.2	20.2-42.7	35.6 \pm 4.1	29.4-42.7	26.9 \pm 2.8	20.2-33.5	0.000
Fat Mass (kg)	DXA	13.6 \pm 4.3	4.7-27.6	12.5 \pm 5.5	6.0-27.6	14.1 \pm 3.6	4.7-22.2	0.153
	Fractionation (1980)	7.8 \pm 2.3	3.7-16.4	7.3 \pm 3.0	4.1-16.4	8.1 \pm 2.0	3.7-13.1	0.076
Fat Mass (%)	DXA	19.0 \pm 5.3	8.7-30.9	15.2 \pm 5.7	9.3-30.9	20.7 \pm 4.1	8.7-30.1	0.000
	Fractionation (1980)	11.5 \pm 3.0	6.1-18.5	9.0 \pm 3.0	6.1-18.5	12.3 \pm 2.4	7.2-18.4	0.000

	Withers (1987)	12.5±4.4	5.5-27.1	10.3±5.1	5.5-27.1	13.5±3.8	5.9-24.7	0.007
	Reilly (2009)	12.6±2.9	7.8-20.9	11.0±3.2	7.8-20.9	13.4±2.4	8.4-19.2	0.001
Indexes (kg/m ²)	Body Mass	23.3±4.4	17.9-30.4	24.6±2.9	20.2-30.4	22.7±2.1	17.9-28.8	0.030
	Fat Mass	4.5±1.4	1.7-8.7	3.9±1.7	2.0-8.7	4.8±1.2	1.7-7.6	0.009
	Fat Free Mass	19.0±2.2	15.6-27.3	21.0±2.4	17.9-27.3	18.0±1.4	15.6-21.5	0.000

406 Data are Mean (μ) \pm Standard Deviation (SD); Minimum (Min); Maximum (Max); DXA=Dual Energy X-Ray Absorptiometry; DXA

407 Fat Free Mass=DXA lean body mass and bone mineral content; Fractionated Fat Free Mass=fractionated muscle mass, fractionated

408 residual mass and fractionated bone mass; Fractionated Lean Body Mass=fractionated muscle mass and fractionated residual mass;

409 Body Mass Index=body mass (kg)/height (m²); Fat Mass Index=DXA fat mass (kg)/height (m²); Fat Free Mass Index=DXA Fat Free

410 Mass (kg)/ height (m²).

411

412 **Table 4. Least square regression analysis of anthropometric models in elite Canadian athletes**

Group	Equation	$\mu \pm SD$ (kg)	Intercept	Slope	SEE	r	M 95% PI*
All N = 64	DXA FFM	57.9±9.9					
	Fract. FFM	60.4±9.0	0.77 (-4.31-4.46)	0.96 (0.89 - 1.03)	2.56	0.96 (0.82 - 1.02)	1.74 (3.49)
	Withers, FFM	61.9±8.7	-5.01 (-8.09-1.93)	1.02 (0.97 - 1.07)	1.70	0.98 (0.90 - 1.03)	1.15 (2.29)
	Reilly, FFM	61.9±8.6	-4.49 (-8.64-0.33)	1.00 (0.94 - 1.07)	2.27	0.97 (0.86 - 1.03)	1.54 (3.08)
	DXA LBM	54.8±8.6					
	Fract. LBM	49.6±7.2	-1.50 (-6.11-3.11)	1.14 (1.02 - 1.23)	2.64	0.95 (0.81 - 1.02)	1.80 (3.60)
	DXA SMM	29.6±5.6					
	Fract. SMM	32.1±5.1	-3.99 (-6.54-(-1.44))	1.05 (0.97 - 1.13)	1.58	0.96 (0.89 - 1.03)	1.57 (3.13)
	Lee, SMM	29.6±5.2	-0.54 (-2.93-1.86)	1.01 (0.94 - 1.10)	1.64	0.96 (0.88 - 1.03)	1.65 (3.30)
Females N = 44	DXA FFM	53.4±5.2					
	Fract. FFM	55.9±5.6	3.71 (-1.91 - 9.31)	0.89 (0.79 - 0.99)	1.80	0.94 (0.84 - 1.05)	1.60 (3.19)
	Withers, FFM	57.9±5.5	0.52 (-4.33-5.38)	0.91 (0.83 - 1.00)	1.50	0.96 (0.87 - 1.05)	1.05 (2.11)
	Reilly, FFM	58.0±5.8	3.54 (-1.80 - 8.87)	0.86 (0.77 - 0.95)	1.72	0.95 (0.85 - 1.05)	1.42 (2.84)
	DXA LBM	50.5±5.0					

	Fract. LBM	46.1±4.6	3.76 (-1.68 - 9.20)	1.02 (0.90 - 1.13)	1.76	0.94 (0.83 - 1.05)	1.65 (3.30)
	DXA SMM	26.9±3.3					
	Fract. SMM	29.7±3.3	-0.87 (-4.54-2.77)	0.94 (0.82 - 1.06)	1.30	0.92 (0.75 - 0.97)	1.07 (2.15)
	Lee, SMM	26.9±2.8	-0.88 (-5.36-3.61)	1.03 (0.87 - 1.20)	1.53	0.89 (0.75 - 1.03)	1.27 (2.54)
Males	DXA FFM	66.7±7.5					
N = 20	Fract. FFM	70.9±7.0	1.12 (-17.66 - 19.89)	0.95 (0.68 - 1.21)	3.80	0.87 (0.63 - 1.11)	2.10 (4.21)
	Withers, FFM	70.9±7.5	-1.12 (-9.08-6.84)	0.97 (0.86 - 1.08)	1.74	0.97 (0.86 - 1.09)	1.37 (2.74)
	Reilly, FFM	70.5±7.6	1.77 (-9.94-13.47)	0.94 (0.77 - 1.10)	2.59	0.94 (0.78 - 1.10)	1.82 (3.64)
	DXA LBM	64.3±7.3					
	Fract. LBM	58.1±5.7	0.49 (-19.19-20.16)	1.11 (0.77 - 1.45)	3.95	0.85 (0.59 - 1.11)	2.16 (4.31)
	DXA SMM	35.6±4.8					
	Fract. SMM	38.0±4.3	-3.32 (-12.72-6.09)	1.02 (0.78 - 1.27)	2.17	0.90 (0.71 - 1.16)	1.38 (2.76)
	Lee, SMM	35.6±4.1	-3.60 (-11.75-4.56)	1.10 (0.87 - 1.33)	1.92	0.92 (0.73 - 1.11)	2.51 (5.02)

413 Data are Mean (μ) \pm Standard Deviation (SD); Fract. = Fractionated; Range in parentheses = 95% interval; M95%PI = mean 95%
414 prediction interval of the DXA-FFM vs Fractionated FFM; DXA-LBM vs Fractionated LBM; DXA SMM vs Fractionated SMM;
415 DXA SMM vs Lee, SMM; r = correlation coefficient; SEE = standard error of the estimate. PI* ranges calculated by multiplying the
416 mean 95% PI interval by 2 (ranges in parentheses).

417 **Table 5. Multiple regression using Withers, Reilly & Lee specified measurement sites and multiple regression with forward**
 418 **selection to develop new ‘Sesbreno’ anthropometric fat free mass and muscle mass equation for elite athletes**

Criterion	Equation	Intercept	Tricep SF	Abd. SF	Thigh SF	Calf SF	Sum 7 SF	Fract. FFM	Fract. FM			R2
DXA FFM	Sesbreno (2019)	3.397 (2.005)						0.975 (0.031)	-0.576 (0.120)			0.94
	Withers (1987)	63.390 (3.278)					-0.077 (0.043)					0.05
	Reilly (2009)	65.539 (2.816)	-0.530 (0.414)	0.373 (0.179)	-0.931 (0.251)	0.874 (0.442)						0.32
Criterion	Equation	Intercept	Height	Age	Sex	Race	C.Arm Girth	C.Thi. Girth	C.Cal. Girth	Fract. SMM	Fract. FM	R2
DXA SMM	Sesbreno (2019)	-2.485 (1.313)								1.058 (0.037)	-0.235 (0.081)	0.93
	Lee (2000)	-36.293 (5.384)	0.270 (3.200)	0.076 (0.043)	0.281 (0.600)	0.021 (0.371)	0.260 (0.002)	0.233 (0.001)	0.258 (0.002)			0.94

419 Sixty-four participants from this study were included; Standard error is shown in parentheses. Abd. = Abdominal, SF = Skinfold
420 (mm), Fract. FFM = Fractionated fat free mass (kg), Fract. FM = Fractionated fat mass (kg), Fract. SMM = Fractionated skeletal
421 muscle mass (kg), C.Arm girth = corrected arm girth (cm), C.Thi girth = corrected mid-thigh girth (cm) and C.Cal girth = corrected
422 calf max girth (cm).